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Control of unsteady wake flows using local oscillation of body surface: a data assimilation study

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Abstract

Variational data assimilation (DA) can expand active flow control techniques to design wall actuators such as synthetic jets or plasma discharges which are difficult to model computationally due to ambiguous boundary conditions at the wall. Here, the control vector for the DA problem is formed by the initial flow and the solid boundary conditions for the body, that means its tangential speed at all times where no particular form is prescribed to the body motion. The control domain takes into account the modeled body surface by means of a direct forcing immersed boundary method (IBM). We consider a configuration of reference flow past a rotationally oscillating cylinder given by Mons & Sagaut, 2017, J. Fluid Mech.. The proposed methodology is applied to the reconstruction of a reference flow generated by a partial control restricted to an upstream part of the cylinder surface as given by Bergmann & Cordier, 2006, Phys. Fluids. DA is also employed to build wall conditions for a direct numerical simulation (DNS) of flow around an airfoil with local oscillation, from synthetic observations of the wake flow downstream the body.

Data assimilation for flow spatio-temporal reconstruction

Goal Provide a DA technique integrating experimental data and DNS to reconstruct the flow dynamics around complex stationary or moving geometries

Control volume technique Force estimation by body wake data assimilation

Partial control on the cylinder surface

 $w_c(\theta_g, t) = \Gamma(\theta_g) A \sin(2\pi f t)$









Boundary forcing estimation through VDA

Problem Recover a system's state X obeying a dynamical law M, given observations at t^* separated by Δt_{obs} $\partial_t X($

$$egin{aligned} \mathbf{x},t) + \mathbb{M}(X(\mathbf{x},t),\eta(t)) &= 0 \ X(\mathbf{x},t_0) &= X_0(\mathbf{x}) + \epsilon(\mathbf{x}) \end{aligned}$$

Dynamical model

$$\nabla \cdot \mathbf{u} = 0$$

$$\frac{\partial \mathbf{u}}{\partial t} = -\nabla p - \frac{1}{2} [\nabla (\mathbf{u} \otimes \mathbf{u}) + (\mathbf{u} \cdot \nabla) \mathbf{u}] + \nu \Delta \mathbf{u} + \mathbf{f}$$

Numerical method \rightarrow Incompact3d

Evaluation of forcing

IBM for simulating flows with moving rigid boundaries Gronskis et al., 2016, Comput. Fluids







Data Assimilation - Cost Functional

 $\begin{array}{c} \mbox{Minimization problem} \\ \mbox{constraint} \Rightarrow \mbox{state dynamics} \Rightarrow \mbox{dependence of the system's state} \end{array}$ variable X on the control variable γ

$$\mathcal{X} \equiv \mathbf{u}(\gamma), \quad \gamma = \{\epsilon(\mathbf{x}), \eta(t)\} \equiv \{\mathbf{u}(\mathbf{x}, t_0), \mathbf{u}(\mathbf{x} ert_{S_B}, t)\}$$

Objective lowest discrepancy between observations and state variable $dx_{obs} > dx$ $J(\gamma) = \int_{t_1}^{t_N} \int_{\Omega_A} \| \overline{\omega}(\mathbf{x}, t) - \omega^{obs}(\mathbf{x}, t) \|_R^2 d\mathbf{x} \Delta_{t^*} dt \\ + \nu(\mathbf{x}) \int_{\Omega_C} \| \overline{\mathbf{u}}(\mathbf{x}, t_0) - \mathbf{u}_{k=0}(\mathbf{x}, t_0) \|^2 d\mathbf{x}$ spatial avg model background state

Control on the Initial and Wall Condition

Flow configuration rotational speed of the cylinder at Re=100: $w_c(t) = A \sin(2\pi ft)$

Vorticity fields at two discrete instants in the assimilation window



Controlled airfoil by arrays of actuators





Conclusion and Outlook

- A new method for reconstructing the flow field from limited measurements where no velocity information is available in a neighborhood of the solid boundary has been introduced.
- Though being restricted to reasonable mesh resolution at the body surface, present technique allows for an accurate pressure reconstruction in a region close to the solid boundary.
- The addition of a penalization term for the wall condition in the cost function will allows us to prevent drastic changes in the temporal solution during the optimization process.
- Introducing a moving boundary cond. as a control parameter will extend VDA to FSI.

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-0.39

-0.59

0.22

0.02

-0.19

-0.39

-0.59

-0.80

2.0 2.5

1.5

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