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#### ORIGINAL PAPER

# Unfolding and refolding properties of S pili on extraintestinal pathogenic *Escherichia coli*

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**Abstract** S pili are members of the chaperone-usherpathway-assembled pili family that are predominantly associated with neonatal meningitis (S<sub>II</sub>) and believed to play a role in ascending urinary tract infections (S<sub>I</sub>). We used force-measuring optical tweezers to characterize the intrinsic biomechanical properties and kinetics of S<sub>II</sub> and S<sub>I</sub> pili. Under steady-state conditions, a sequential unfolding of the layers in the helix-like rod occurred at somewhat different forces, 26 pN for S<sub>II</sub> pili and 21 pN for S<sub>I</sub> pili, and there was an apparent difference in the kinetics, 1.3 and 8.8 Hz. Tests with bacteria defective in a newly recognized sfa gene (sfa $X_{\rm II}$ ) indicated that absence of the sfa $X_{\rm II}$  gene weakens the interactions of the fimbrium slightly and decreases the kinetics. Data of S<sub>I</sub> are compared with those of previously assessed pili primary associated with urinary tract infections, the P and type 1 pili. S pili have weaker layer-to-layer bonds than both P and type 1 pili, 21, 28 and 30 pN, respectively. In addition, the S pili kinetics are  $\sim 10$ times faster than the kinetics of P pili and  $\sim 550$  times faster than the kinetics of type 1 pili. Our results also show

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that the biomechanical properties of pili expressed ectopically from a plasmid in a laboratory strain (HB101) and pili expressed from the chromosome of a clinical isolate (IHE3034) are identical. Moreover, we demonstrate that it is possible to distinguish, by analyzing force-extension data, the different types of pili expressed by an individual cell of a clinical bacterial isolate.

**Keywords** Fimbriae · Uropathogenic *Escherichia coli* · Bond breaking · Unfolding · Optical tweezers

#### Introduction

Extraintestinal pathogenic Escherichia coli (ExPEC) are known to be able to express a variety of flexible adhesion organelles, referred to as pili or fimbriae. Even though each single bacterium has the potential to express several different pili, it seldom produces more than one type of pili simultaneously presumably because of regulation in response to signals from the surrounding environment (as reviewed by Holden and Gally 2004). A rationale for the bacterium to express several types of pili is that different pili bind to different receptors expressed on the host tissue. For example S, P, and type 1 fimbrial adhesins specifically recognize α-sialyl-2,3-galactose (Parkkinen et al. 1986),  $Gal(\alpha 1-4)\beta Gal$  (Lund et al. 1987), and  $\alpha$ -D-mannoside receptors (Old 1972), respectively. Recent studies have shown that the adhesive potential of bacteria is not solely given by the properties of the adhesin molecules located at the distal end of the adhesion organelles; it can be strongly influenced also by the biomechanical properties of the pilus shaft structure constituting the main part of adhesion organelles (Duncan et al. 2005). A full understanding of bacterial adhesion therefore requires that we improve our



knowledge about both the biomechanical and adhesive properties of attachment organelles.

The most studied pili, P pili (pyelonephritis-associated pili) and type 1 pili, characterized with respect to their three-dimensional structure and intrinsic mechanical properties (Andersson et al. 2007; Fällman et al. 2005), are commonly found on uropathogenic *E. coli* (UPEC). It has recently been shown that these helix-like structures,  $\sim$ 7-nm thick and  $\sim$ 1–2- $\mu$ m long, possess large flexibility, mainly originating from their quaternary architecture (Jass et al. 2004). The quaternary structure is assembled from  $\sim$ 10<sup>3</sup> subunits that are linked head-to-tail via a donor strand exchange where the subunit donates its amino terminal extension to complete the fold of its neighbor (Sauer et al. 1999). These subunits are ordered in a helix-like sequence where the layer is connected to an adjacent layer via layer-to-layer interactions.

The quaternary structure of the pilus can be unfolded by unzipping the layers and thereby elongating the fimbrium. This action helps several pili share the shear forces caused by, e.g., the rinsing action of the urine, and it is hypothesized that this property controls the load on the adhesin and thereby optimizes the bond lifetime of, for instance, the FimH-mannose (Forero et al. 2006) and the PapG-galabiose (Björnham et al. 2009) interactions. If the action is performed under steady state, the unfolded structure can refold to its original configuration without dissipating energy (Andersson et al. 2008). The unfolding/refolding can also be a repeat action, meaning that the pili may be suggested to work as active dampers for shear forces (Andersson et al. 2006b). We have previously defined the extension behavior, i.e., the unfolding response to force by designating three separate regions that give rise to distinct differences in behavior (Andersson et al. 2008; 2006c; Jass et al. 2004). The first extension response (region I) shows a linear increase in force that indicates an elastic stretching of the layers. The second part (region II) corresponds to the unzipping of the layers that gives rise to a constant forceextension response. The third part (region III) shows a pseudo-elastic response that is similar to a worm-like chain model including a phase transition of the individual units that gives a smooth transition in the force-extension curve.

S pili can bind to human bladder and kidney epithelium and are predominantly correlated with neonatal meningitis caused by newborn meningitis  $E.\ coli$  (NMEC). In addition, they are also found in UPEC isolates and may have a role in ascending urinary tract infections (Wright and Hultgren 2006). S pili are expressed from polycistronic gene clusters, and the  $sfa_I$  and  $sfa_{II}$  pili operons characterized in ExPEC strains 536 (Berger et al. 1982; Hacker et al. 1985) and IHE3034 (Hacker et al. 1993) represent cases of S pili associated with urinary tract infection and meningitis, respectively. In spite of slightly different amino

acid compositions of the respective subunits in the operons, both variants of S pili recognize the  $\alpha$ -Sialyl-2,3-galactose receptor. In the quest of extending the knowledge about the physical properties and the divergence among different pili expressed by ExPEC, we have characterized the mechanical behavior of the two different S pili with force-measuring optical tweezers (FMOT). The high-force resolution of FMOT allows for detailed characterization of a single pilus, whereby we can assess the kinetics at a single polymer level. Prompted by the difference in kinetics observed for P and type 1 pili, we set out to characterize the properties of S pili to enable a comparison with P and type 1 pili, whose biogenesis, structure, and biological functions nevertheless are similar (Berglund and Knight 2003; Knight et al. 2002).

#### Materials and methods

#### Bacterial strains

The *E. coli* strains used in this study are shown in Table 1. The strains were grown at 37°C on solid L broth containing 1.5% agar, complemented with carbenicillin, Cb (50  $\mu$ g/ml), when necessary. The clinical isolate was grown statically in brain-heart infusion (BHI) medium at 37°C when type 1 fimbriation was examined.

#### Construction of plasmids

Molecular genetics manipulations were performed essentially as described by Sambrook et al. (Sambrook and Russel 2001). The *Bam*HI-*Sal*I fragments with the  $sfaX_{II}$  mutated genes from both pASS1 and pASS4 plasmids were cloned into the suicide vector pKO3. The resulting plasmids were introduced into MG1655/pAZZ50. As described by Guzman et al. (1995), the resulting plasmids pAES7 ( $sfaX_{II}$ ::kan) and pAES8 ( $\Delta sfaX_{II}$ ) were obtained by homologous recombination.

#### Atomic force microscopy (AFM)

Imaging of bacterial pili using AFM was done essentially as described earlier with some modifications (Balsalobre et al. 2003). Bacterial cells from solid medium were suspended in 50  $\mu$ l filtered water before 10  $\mu$ l was placed onto freshly cleaved ruby red mica (Goodfellow Cambridge Ltd, Cambridge, UK). The cells were incubated for 5 min at room temperature and blotted dry before being placed into a dessicator for a minimum of 2 h. Images were collected in a Nanoscope V AFM (Veeco software) using Tapping-Mode TM with standard silicon cantilevers oscillated at resonant frequency (270–305 kHz). Images were collected



Table 1 Strains and plasmids used in this study

Plasmids and strains	Relevant characteristics	References	
IHE3034	NMEC clinical isolate, O18K1:H7, carrier of the $sfa_H$ operon (S pili)	Korhonen et al. (1985)	
HB101	Non-piliated	Boyer and Roulland (1969)	
MG1655	$F^-$ ilv $G$ rph $I$	Guyer et al. (1980)	
pAZZ50	sfa <sub>II</sub> operon (S pili) from the NMEC clinical isolate IHE3034 cloned into pBR322, Cb <sup>R</sup>	Hacker et al. (1993)	
pANN801-13	$sfa_I$ operon (S pili) with truncated $sfaX_I$ gene from the UPEC clinical isolate 536 cloned into pBR322, Cb <sup>R</sup>	Hacker et al. (1985)	
pPAP5	pap operon (P pili) from the UPEC clinical isolate J96 cloned into pBR322, Cb <sup>R</sup>	Lund et al. (1988)	
pPKL4	fim operon (type 1 pili) from E. coli K12 PC31 cloned into pBR322, Cb <sup>R</sup>	Klemm et al. (1985)	
pKO3	Suicide vector, ori M13, sacB, repA <sup>TS</sup> , Cm <sup>R</sup>	Guzman et al. (1995)	
pASS1	pUC18, sfaX <sub>II</sub> ::kan, Cb <sup>R</sup> , Km <sup>R</sup>	Sjöström et al. (2009a)	
pASS4	pUC18, $\Delta sfaX_{II}$ , $Cb^{R}$	Sjöström et al. (2009a)	
pAES7	$pAZZ50$ , $sfaX_H::kan$ , $Cb^R$ , $Km^R$	This work	
pAES8	pAZZ50, $\Delta sfaX_{II}$ , Cb <sup>R</sup>	This work	

in air at a scan rate of approximately 0.5–1.5 Hz. The final images were flattened and/or plane fitted in both axes using Veeco software and presented in either height or amplitude (error) mode.

Sample preparation and optical tweezers force measurements

We used force-measuring optical tweezers to extend an individual pilus under both steady-state conditions and during dynamic force spectroscopy (DFS) measurements. Several extension/contraction and DFS measurements were performed with an experimental procedure under standardized conditions that earlier has been used for characterization of P and type 1 pili (Andersson et al. 2006a, c; Fällman et al. 2004). In a given bacterial sample, individual pili were stretched from different bacteria with a 3.0-µm semi-transparent bead that acted as a force transducer. All beads were individually calibrated prior to each single pilus measurement. Measurements were repeated with each bacterial strain on different occasions, and data sets from at least three separate experiments were collected. Unfolding forces and their respective standard deviations were obtained for each experiment.

#### Theory of unfolding a helix-like polymer

A detailed description of the force-extension behavior of pili is found in (Andersson et al. 2006c). However, a brief summary is given below. As mention above, pili are assembled from many subunits into a helical arrangement. In addition, the quaternary structure is held rigid via layer-to-layer bonds, whereas head-to-tail interactions create the

backbone. This structural design gives a response to external forces that is different from those of other macromolecules. The main rod is made from the major subunits: SfaA, PapA, and FimA, for S, P, and type 1 pili, respectively (Knight et al. 2002). Unfolding of the rod at an arbitrary position in the interior of the rod is very improbable since this requires the opening of several bonds simultaneously (Andersson et al. 2008). Consequently, the rod will unfold in a sequential manner after an initial fracture. The net opening rate of the outermost bond and the force-extension behavior are well described via rate theories and a sticky-chain model (Andersson et al. 2006a, c). The rate equation for such opening under a force, F, is given as,

$$dN_{\rm B}/dt = k_{\rm AB}^{\rm th} e^{F\Delta x_{\rm AT}/kT} - k_{\rm AB}^{\rm th} e^{(\Delta V_{\rm AB} - F\Delta x_{\rm TB})/kT}, \tag{1}$$

where  $k_{\rm AB}^{\rm th}$  is the thermal bond opening rate,  $\Delta x_{\rm AT}$  and  $\Delta x_{\rm TB}$  are the bond lengths, i.e., the distance from the closed and open state to the transition barrier, and  $\Delta V_{\rm AB}$  is the bond energy. Finally, k is the Boltzmann factor and T the temperature. For steady-state conditions, the opening and closure rates are at balance, which leads to an analytic solution for the steady-state unfolding force,  $F_{\rm LIF}^{\rm bal}$ ,

$$F_{\rm UF}^{\rm bal} = \Delta V_{\rm AB} / \Delta x_{\rm AB}, \tag{2}$$

where  $\Delta x_{\rm AB}$  is the bond opening length of the layer-to-layer bond (Andersson et al. 2006c). For high extension speeds the refolding rate in Eq. 1 can be neglected, and the rate equation simplifies to an expression relating the unfolding force to the extension speed,  $\dot{L}$ , as

$$F_{\rm UF}(\dot{L}) = kT/\Delta x_{\rm AT} \ln(\dot{L}/\dot{L}^{\rm th}),\tag{3}$$

where  $\dot{L}^{th}$  is defined to be the *thermal extension speed*, given by  $k_{AB}^{th} \Delta x_{AB}$  (Andersson et al. 2006a). It is thereby



possible to use unfolding force-extension speed data to assess characteristic properties of the pilus under study, e.g., the bond length and the thermal extension speed.

These parameters can be assessed via dynamic force spectroscopy measurements (DFS), where the pilus is extended a number of times at different speeds (Andersson et al. 2006a), or via relaxation experiments (Andersson et al. 2007), where the pilus is forced to respond with a high force through an extension at high speed after which the extension is halted and the relaxation process is analyzed. In DFS characterizations, the unfolding force is described by Eq. 3, whereas the relaxation process is described by

$$dF_{\rm UF}(t)/dt = -\dot{L}^{\rm th}\kappa(e^{F_{\rm UF}(t)\Delta x_{\rm AT}/kT} - e^{(\Delta V_{\rm AB} - F_{\rm UF}(t)\Delta x_{\rm TB})/kT}), \tag{4}$$

where  $\kappa$  is the elastic constant of the force transducer (Andersson et al. 2007). In this work we use both these methods to assess the specific parameters of the different S pili and compare them with the parameters assessed for P and type 1 pili (Andersson et al. 2007).

#### Results and discussion

Expression of S pili variants by E. coli

S pili are expressed by pathogenic E. coli and two different variants, Sfa<sub>I</sub> and Sfa<sub>II</sub> (here referred to as S<sub>I</sub> and S<sub>II</sub> pili, respectively), have been extensively studied by molecular genetics approaches in case of the ExPEC strains 536 (Berger et al. 1982; Hacker et al. 1985) and IHE3034 (Hacker et al. 1993). The gene organization and functions of the genes in the two sfa operons are the same, but there are some sequence differences at both DNA level and amino acid level (Fig. 1a,b). Interestingly, the pili biogenesis components (e.g., the SfaE chaperon and SfaF usher proteins) residing inside the bacterium are almost identical (96-100%), whereas the structural fimbrial subunits and the adhesin, i.e., SfaA, SfaH, and SfaS, exposed outside the bacterium show differences of 16-40%. As is shown in Fig. 1b, an alignment of the major structural pilus subunit sequences, the SfaA<sub>I</sub> and SfaA<sub>II</sub> subunits, reveals that there is a  $\sim 20\%$  difference at the amino acid level, whereas the SfaX<sub>I</sub> and SfaX<sub>II</sub> proteins are identical with the exception of only 2 out of 166 amino acid residues.

Force measurements on pili expressed by the clinical isolates IHE3034

The clinical *E. coli* isolate strain IHE3034 carries the genes to express S<sub>II</sub>, MatB, and type 1 pili (Korhonen et al. 1985; Pouttu et al. 2001; Selander et al. 1986). We grew this

strain to promote expression of either S<sub>II</sub> or type 1 pili and used FMOT to investigate and assess specific intrinsic parameters of the expressed pili. The studies on the IHE3034 strain were performed in the same way as earlier described by Andersson et al. (2007). By identifying parameters such as steady-state response and kinetic behavior, at the single pilus level, a typical set of curves was obtained. As can be seen in the right panels of Fig. 2a,b, two different curve profiles appeared. By comparing the force responses and parameter values to previously assessed curves of HB101/pPKL4, it was obvious that the curve in panel A corresponded to a type 1 pilus (Andersson et al. 2007). The large gap between the unfolding and refolding plateau indicates, as also mentioned in (Andersson et al. 2007), that the experiment is not performed at steady state. In addition to the curve in panel A, we suggested that the curve in panel B was a representation of an S pilus. The average unfolding force of the presumed type 1 pili expressed by the IHE3034 strain, shown in Fig. 2a and fitted with a Gaussian function, was assessed to  $55 \pm 4$  pN, whereas the presumed unfolding force of  $S_{II}$  pili was assessed to 26  $\pm$  1 pN. Pili expressed by the second isolate were also analyzed with immunoglobulin antibody labeling to verify the FMOT results with respect to actual presence of the S pili on the bacteria (data not shown).

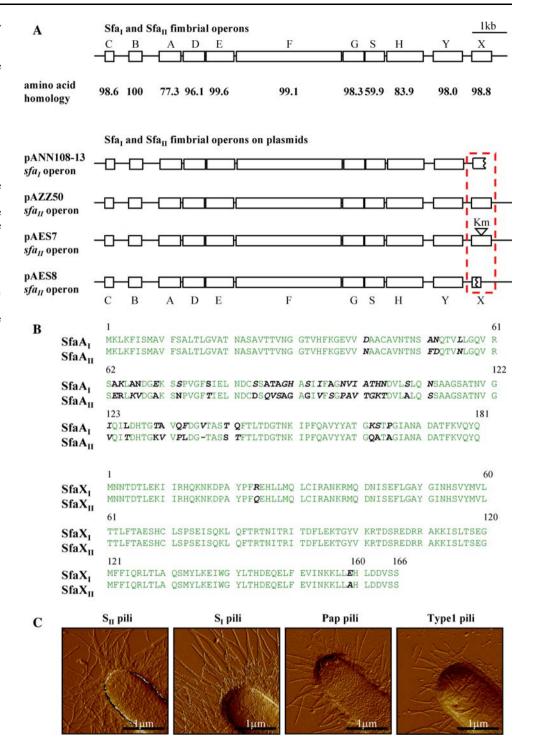
#### Characterization of S pili under steady-state

In order to specifically examine and compare the properties of each type of pili in a common genetic background, we used the *E. coli* laboratory strain HB101 (that lacks genes for pilus biogenesis) as host for plasmids harboring fimbrial gene clusters cloned from different ExPEC isolates. Figure 1c shows four representative areas of HB101 bacteria expressing S<sub>I</sub>, S<sub>II</sub>, P, and type 1 pili, visualized with atomic force microscopy (AFM). From the images, it could be concluded that all pili were expressed ectopically in the host strain and that no distinct differences considering lengths and number expressed per cell could be observed.

A typical force-extension/contraction response of  $S_{II}$  pili expressed from the plasmid-borne  $sfa_{II}$  gene cluster (HB101/pAZZ50) under steady-state conditions is shown in the right panel of Fig. 2c. The data (black curve) represent (I) stretching of the coiled SfaA<sub>II</sub> rod, (II) sequential opening of the layer-to-layer bonds, and (III) transitions of the head-to-tail bonds. Such a response was similar to those assessed for P and type 1 pili (Andersson et al. 2007; Lugmaier et al. 2008; Miller et al. 2006). The average steady-state unfolding force, i.e., the force required to break the layer-to-layer bonds between consecutive layers, was found to be  $26 \pm 1$  pN, which is slightly lower than the values for P and type 1 pili,  $28 \pm 2$  pN and  $30 \pm 2$  pN,



Fig. 1 a A schematic overview of the  $sfa_I$  and  $sfa_{II}$  fimbrial chromosomal operons [compilation based on sequence data and annotations (NCBI GenBank: CP000347: Brzuszkiewicz et al. 2006: Sjöström et al. 2009b)] and the  $sfa_I$ ,  $sfa_{II}$ ,  $sfaX_{II}$ ::kan, and  $\Delta sfaX_{II}$  plasmid borne operons. The calculated homology in percent at amino acid level is shown under the drawings of the chromosomal genes. The different alleles of the sfaX gene in the plasmid borne operons are highlighted by the red box. b Multiple sequence alignment (Corpet 1988) of the SfaA<sub>I</sub> and SfaA<sub>II</sub> major fimbrial subunit proteins (uppermost) and of the  $SfaX_I$  and  $SfaX_{II}$  (lowermost). Green residue combinations are identical. c AFM micrographs showing the different pili described in this study. The scanned area for each image was 5 by 5  $\mu$ m<sup>2</sup>



respectively (Andersson et al. 2008). Thus, the force required to break the layer-to-layer bonds are similar to that assessed for the clinical isolate cultured for S pili. The right panel of Fig. 2c shows multi-pili attachment to the bead. When separating the bacteria-bead system gently, the shortest and weakest attached pili will detach. Initially, four pili are attached, whereafter three detach, each event indicated with  $a + \mathrm{sign}$ .

The green and red curves show two consecutive contraction patterns that represent refolding of the extended structure to its native form. As already shown for P and type 1 pili, refolding to the native form requires the formation of a nucleation kernel (Fällman et al. 2005; Lugmaier et al. 2008), i.e., after a pilus has been extended to a linearized form, it needs a certain amount of slack to reform the layer-to-layer interactions (Lugmaier et al. 2008). The sequential



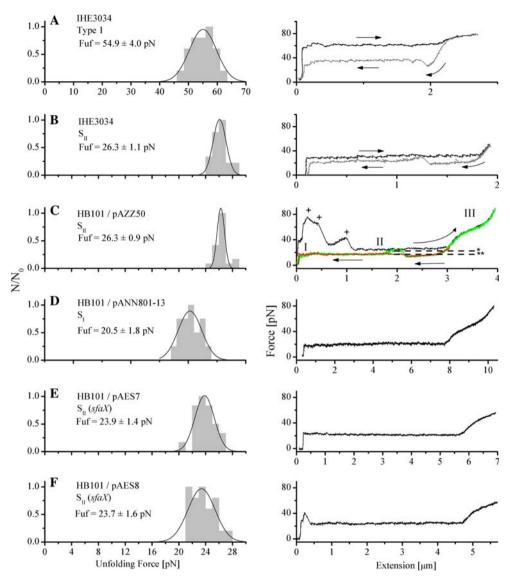


Fig. 2 Characterization of pili with force-measuring optical tweezers. The left side panels show the unfolding forces fitted with a Gaussian function (normalized distributions) for each respective strain. The right side panels represent force measurements of **a** wild-type bacteria IHE3034 expressing type 1 pili (black curve, unfolding; grey curve, refolding) and **b** wild-type bacteria IHE3034 expressing S pili (black curve, unfolding; grey curve, refolding). These two sets of curves do not show a complete region III response. The arrows indicate the direction of the applied force, i.e., the right pointing arrow indicates elongation, whereas the left pointing arrow indicates

contraction of the pili. c A typical response from an S pilus, HB101/pAZZ50, under steady-state conditions. The *black curve* represents the unfolding sequence (the *initial peaks*, marked by +, are due to multi-pili interaction). The *red* and *green* (partly overlapping) *curves* show two consecutive refolding sequences. The characteristic unfolding regions I, II, and III are marked in the figure, and the two possible refolding levels are marked by \* and \*\*. d Unfolding response of the UTI correlated pili HB101/pANN801-13. *Panels E* and *F* are the unfolding responses of HB101/pAES7 and HB101/pAES8 pili, respectively

refolding can continue until all subunits are organized into a structure with the original helix-like shape. As shown in Fig. 2c, there was a distinct increase in force of  $\sim 10$  pN at  $\sim 2.1$  µm that indicated the creation of a nucleation kernel. Moreover, like the structure of type 1 pili, the S<sub>II</sub> pili could refold at two different force levels, which is an indication of two possible configurations (Andersson et al. 2007). In the first cycle the pilus refolded at a force of  $\sim 18$  pN (Fig. 2c; red line curve plot level marked with \*\*), whereas in the

subsequent cycle it initially refolded at  $\sim 23$  pN (Fig. 2c; green line curve plot level marked with \*) until it had contracted to  $\sim 1.8$  µm. The refolding force then dropped and remained at  $\sim 18$  pN.

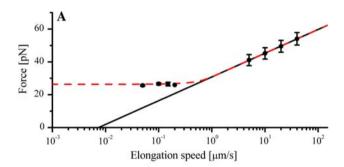
To elucidate if there would be any detectable difference between S pili correlated to UTI and NMEC, we performed force-extension and kinetic response measurements of S<sub>I</sub> pili encoded from the pANN801-13 plasmid clone. Not surprisingly, since the fimbrial components at protein level

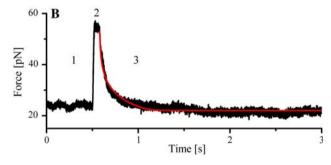


and the presumed pili polymer architecture are almost identical, the force-extension under steady state appeared similar. A force-extension response from the  $S_I$  pili measurements is plotted in Fig. 2d, right panel. However, interestingly the average steady-state unfolding force was assessed to be 21  $\pm$  2 pN, which is lower in comparison to that of the  $S_{II}$  pili.

## Characterization of S pili with dynamic force spectroscopy

In order to find specific intrinsic parameters of these pili, we performed DFS measurements (Andersson et al. 2006a). The bond length of the layer-to-layer bonds,  $\Delta x_{\rm AT}$ , and the corner velocities,  $\dot{L}^*$ , i.e., the extension speed above which the pilus shows a dynamic behavior, were analyzed. In the experiments, the unfolding region of a pilus was extended at 5, 10, 20, and 40 µm/s over a distance of 3 µm (Andersson et al. 2006a). The average unfolding forces of  $S_{\rm II}$  are plotted and fitted to Eq. 3 (solid line), see Fig. 3a. Since the  $S_{\rm II}$  pili can be extended under steady-state conditions for velocities under  $\sim 0.4$  µm/s, four data points are inserted in the figure for representative purpose. These are, however, not included in the fit.





**Fig. 3 a** Dynamic force spectroscopy measurement of  $S_{II}$  pili. The rod was unfolded at 5, 10, 20, and 40 µm/s over a distance of 3 µm. The average fit of all data with Eq. 3 gave a bond length of  $0.66 \pm 0.08$  nm and a corner velocity of  $450 \pm 150$  nm/s. Unfolding forces taken under steady-state conditions (velocities <0.2 µm/s) are also included, and the *dashed red line* is a numeric simulation of Eq. 3 in (Andersson et al. 2006a). **b** The data were sampled during a relaxation measurement and fitted to Eq. 4. For this particular set of data, the bond length and the thermal bond opening rate of the subunits were assessed to 0.67 nm and 1.3 Hz, respectively

The average bond lengths of  $S_{II}$  and  $S_{I}$  pili were assessed to  $0.66\pm0.08$  nm and  $0.56\pm0.14$  nm, whereas the corner velocities were found to be  $450\pm150$  nm/s and  $700\pm100$  nm/s, respectively. The thermal bond opening rates were in turn assessed to  $1.3\pm0.9$  Hz and  $8.8\pm5.3$  Hz. Thus, the kinetics of  $S_{I}$  is  $\sim7$  times higher than for  $S_{II}$ . These parameters are in the same regime as those assessed for P pili, i.e.,  $0.76\pm0.11$  nm,  $400\pm100$  nm/s, and  $0.8\pm0.5$  Hz, respectively (Andersson et al. 2006a). The corner velocity and thermal bond opening rate are on the other hand significantly different from those of type 1 pili,  $6\pm3$  nm/s and  $0.016\pm0.009$  Hz, whereas the bond length is similar,  $0.59\pm0.06$  nm (Andersson et al. 2007).

To further illustrate kinetic divergences among pili, we performed relaxation measurements (Andersson et al. 2007). A typical relaxation process for an  $S_{\rm II}$  pilus, extended under dynamic conditions, is shown in Fig. 3b. The measurement procedure was performed in the following sequence (1) the pilus is at steady state; (2) the pilus is extended at 40  $\mu$ m/s, i.e., above the steady-state extension speed; (3) the extension is halted, whereafter the pilus relaxes to balance force. This method gives similar results as DFS measurements but visualizes the kinetic behavior of pili in an illustrative way. With a fit to Eq. 4, this particular curve gave a bond length and thermal bond opening rate of  $0.66 \pm 0.08$  nm and  $1.3 \pm 0.9$  Hz, which is in line with the parameter values assessed through DFS measurements.

As mentioned above, we assumed that the curve in Fig. 2b, right panel, represented a force-extension response of a S<sub>II</sub> pilus from the IHE3034 bacteria. It was found that the average steady-state unfolding force of the pili expressed by that strain was  $26 \pm 1$  pN. This is identical with the results presented above for  $S_{\rm II}$  pili expressed by HB101/pAZZ50. In addition, the bond length and thermal bond opening rate were assessed to  $0.66 \pm 0.08$  nm and  $0.8 \pm 0.4$  Hz in the clinical isolate in comparison to  $0.66 \pm 0.08$  nm and  $1.3 \pm 0.9$  Hz for HB101/pAZZ50expressed pili. We can therefore deduce that S<sub>II</sub> pili expressed by two different strains—IHE3034 expressing  $S_{II}$  from the chromosome and HB101/pAZZ50 expressing S<sub>II</sub> ectopically—show identical properties. Thus, the measurements indicate that the biomechanical properties of pili are not changed if the operons for pili biogenesis of a clinical isolate are implemented into the HB101 strain via a plasmid. It is therefore justified to use strain HB101 as a common model system for comparative studies of different pili types in a uniform strain background.

Differences in unfolding-refolding kinetics among different S pili

The  $S_I$  and  $S_{II}$  pili are encoded from operons that are highly homologous, and it was an interesting observation that they



Table 2 Parameter values of S, P, and type 1 pili

Strain	IHE3034	IHE3034	HB101	HB101	HB101	HB101	HB101	HB101
Plasmid	_	_	pAZZ50	pANN801-13	pAES7	pAES8	pPAP5	pPKL4
Pili	$S_{II(wt)}$	Type 1 <sub>(wt)</sub>	$S_{II}$	S <sub>I(sfaX truncated)</sub>	$S_{II(sfaX::kan)}$	$S_{II(\Delta sfaX)}$	$P^{a}$	Type 1 <sup>b</sup>
$F_{uf} \left( pN \right)^c$	$26 \pm 1$	$32 \pm 3$	$26 \pm 1$	$21 \pm 2$	$24 \pm 1$	$24 \pm 1$	$28 \pm 2$	$30 \pm 2$
Exp. I	$28 \pm 1$		$26 \pm 1$	$19 \pm 1$	$24 \pm 1$	$25 \pm 1$		
Exp. II	$26 \pm 1$		$27 \pm 1$	$22 \pm 1$	$24 \pm 2$	$25 \pm 1$		
Exp. III	$26 \pm 1$		$27 \pm 1$	$20 \pm 1$	$24 \pm 1$	$23 \pm 1$		
$\Delta V_{\mathrm{AB}} \; (kT)$	$35 \pm 5$	$40 \pm 7$	$37 \pm 5$	$28 \pm 5$	$33 \pm 5$	$33 \pm 5$	$24 \pm 1$	$37 \pm 2$
$\Delta x_{\rm AT}$ (nm)	$0.66\pm0.08$	$0.56 \pm 0.03$	$0.66\pm0.08$	$0.56 \pm 0.14$	$0.74 \pm 0.09$	$0.67 \pm 0.04$	$0.76 \pm 0.11$	$0.59 \pm 0.06$
$k_{\mathrm{AB}}^{\mathrm{th}}$ (Hz)	$0.8\pm0.4$	$0.012 \pm 0.004$	$1.3 \pm 0.9$	$8.8 \pm 5.3$	$0.8 \pm 0.5$	$0.9 \pm 0.6$	$0.8 \pm 0.5$	$0.016 \pm 0.009$
<i>L</i> * (nm/s)	$200\pm50$	$6\pm2$	$450\pm150$	$700\pm100$	$280\pm70$	$220\pm50$	$400\pm100$	$6\pm3$

<sup>&</sup>lt;sup>a</sup> References (Andersson et al. 2006a, c)

showed a difference regarding the force needed to rupture the layer-to-layer interaction in the rod and a seven-fold difference in kinetics. One possible reason for these differences could be that the few differences in amino acid sequence of the SfaA pilin subunits would have an impact on the biophysical properties monitored here. An alternative possibility became evident when we examined the Sfa clones in more detail and found-by nucleotide sequencing of the distal end of the  $sfa_I$  gene cluster in plasmid pANN801-13-that it is lacking about 40% of the  $sfaX_I$  gene in contrast to the pAZZ50 clone that carries a complete gene cluster including the  $sfaX_{II}$  gene (Fig. 1b). Both clinical isolates carry intact sfaX alleles in the sfa operons on their chromosomes,  $sfa_I$  in case of the UPEC isolate 536 (Brzuszkiewicz et al. 2006) and  $sfa_{II}$  in case of the NMEC isolate IHE3034 (Sjöström et al. 2009b). The  $sfaX_{II}$  gene has recently been shown to be part of the major sfa gene operon (Sjöström et al. 2009b). The SfaX protein belongs to a family of MarR-like regulatory proteins. Our studies have shown that expression of the  $sfaX_{II}$  gene affects motility by down regulation of flagella biosynthesis, and similar findings were reported for the largely homologous papX gene of a UPEC strain (Simms and Mobley 2008; Sjöström et al. 2009a). It was also found that  $sfaX_{II}$ expression affected the DNA phase variation process leading to OFF status of the type 1 fimbrial expression (Sjöström et al. 2009a). However, while no effect on the expression of S<sub>II</sub> pili was detected, its potential role for some steps in pili biogenesis, by being a part of the S<sub>II</sub> pili operon, has not been ruled out (Sjöström et al. 2009b). This prompted us to directly test if expression of the  $sfaX_{II}$  gene might affect the biomechanical features and the physical properties of the pili and thereby be a component involved in the differences observed between  $S_{\rm I}$  and  $S_{\rm II}$  pili.

Therefore, we constructed mutant derivatives of the  $S_{II}$  piliclone such that we could perform measurements with pilicexpressed from bacteria lacking the  $sfaX_{II}$  gene.

The plasmids pAES8 and pAES7 are identical to pAZZ50 except that the  $sfaX_{II}$  gene is mutated either by partial deletion or by a Km-cassette insertion, respectively (Fig. 1b). Force-extension measurement, see Fig. 2e,f, right panels, of pili expressed by the two  $sfaX_{II}$  mutated variants indicated that the average steady-state unfolding force was  $24 \pm 1$  pN and  $24 \pm 2$  pN, respectively. The thermal bond opening rate and the bond length were assessed to  $0.9 \pm 0.6$  Hz,  $0.67 \pm 0.04$  nm and  $0.8 \pm 0.5$  Hz,  $0.74 \pm 0.09$  nm, respectively.

As is shown in Table 2, there was good reproducibility in the experiments performed on different occasions, and the results indicate that there could be minor biomechanical differences between the  $S_{II}$  pili expressed from the  $sfaX_{II}$ gene mutant derivatives and from the complete (pAZZ50) clone. The latter unfolded at  $26 \pm 1$  pN with a thermal bond opening rate of  $1.3 \pm 0.9$  Hz and a bond length of  $0.66 \pm 0.08$  nm. It is not ruled out that the difference observed might be due, for example, to a regulatory role of the SfaX protein that might affect the biogenesis at the level of subunit stoichiometry and/or the assembly process. Recent findings regarding the role of SfaX in regulation at the transcriptional level of type 1 pili and flagella expression suggest that it is unlikely that the SfaX<sub>II</sub> protein would be incorporated into the S<sub>II</sub> pili structures (Sjöström et al. 2009a). The  $sfaX_{II}$  gene product shows homology to other regulatory proteins possessing DNA-binding properties, and its predicted secondary structure appears different from the S pili subunit proteins (data not shown). It remains to be elucidated at what level the SfaX proteins possibly may affect the S pili biomechanical properties.



<sup>&</sup>lt;sup>b</sup> Reference (Andersson et al. 2007)

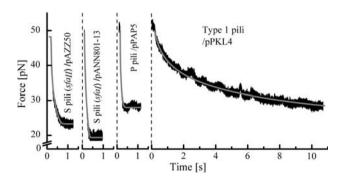
<sup>&</sup>lt;sup>c</sup> Mean values of data from at least three experiments as described in Fig. 2. To illustrate the reproducibility we show the individual data sets from three separate experiments (Exps. I–III) in case of the S pili measurements

#### Difference of unfolding/refolding dynamics among pili

As assessed previously and in this work, pili of the helixlike family show similar force-extension/contraction responses attributable to the geometrical shape and the similarity of the subunits. However, the force needed to unravel the quaternary structures and the dynamics of pili are slightly different. A comparison of the kinetics and the steady-state force of P, type 1, S<sub>I</sub>, and S<sub>II</sub> pili is shown in Fig. 4. As seen in the figure, they show major differences in their relaxation behavior, i.e., the transition time from a dynamic to a steady-state force response. The kinetics of S<sub>I</sub> and S<sub>II</sub> pili are similar to P pili, but the steady-state forces are lower. However, for type 1 pili the kinetics are significantly slower, whereas the steady-state force is slightly higher in comparison to the other three. We have summarized in Table 2 the results of this study and the parameter values assessed from our earlier studies of P and type 1 pili.

#### Comparison between SfaA<sub>I</sub> and SfaA<sub>II</sub>

The small genetic variation between SfaA<sub>I</sub> and SfaA<sub>II</sub>,  $\sim 20\%$ , and the identical three-dimensional helix-like structure point towards minor differences in the biomechanical properties. Using force-measuring optical tweezers in situ measurements, we have shown that the force-extension response of these two fimbria is identical. They can be unfolded to a linearized polymer and reversibly be refolded back to its original structure. This action can be performed without any indication of plasticity or fatigue that is similar to P pili (Andersson et al. 2006b). However, the force required to unravel the helix-like structures (quaternary) is slightly dissimilar.  $S_{II}$  pili expressed by NMEC seem to have stronger layer-to-layer interactions compared to  $S_{I}$  pili expressed by UTI.



**Fig. 4** Relaxation data curves from  $S_I$ ,  $S_{II}$ , P, and type 1 pili fitted with Eq. 4. Each set of data is plotted with an individual X-axis (abscissa) with a truncated Y-axis. Data for P pili and type 1 pili were taken from earlier published results (Andersson et al. 2006a, c; Andersson et al. 2007). Differences in the kinetic behavior and the final steady-state force level are clearly seen

It has been shown, and is further discussed below, that E. coli expressing type 1 pili increases its adhesion time when exposed to shear forces induced by a flow (Thomas et al. 2002). Also, it is believed that the shaft of the pilus has coevolved with the adhesin for optimized performance. Thus, we suggest that a difference in unraveling force of the two S pili might be correlated to in vivo environmental forces generated by natural flows, such as urine and blood flows. Moreover, the kinetic differences, i.e., the speed at which a subunit in the helix-like rod opens/closes, of the two pili can presumably be addressed to the variation in shear flow rates within the urinary tract or blood-brain barrier. However, verifying this hypothesis requires detailed information regarding the in vivo shear forces and shear rates that can improve the knowledge regarding how the development and expression of pili helps bacteria to optimize adhesion under different environmental conditions. For such a study, S<sub>I</sub> and S<sub>II</sub> pili, which are correlated to different in vivo environments, could be a suitable model system since they have been characterized with respect to their genetic and structural compositions and now also for their force and kinetic responses.

We also wish to point out that this work verifies that pili encoded from a unique operon but expressed by two different bacterial strains (the clinical isolate IHE3034 and the laboratory strain HB101) do not show any biomechanical differences in terms of bond length, steady-state unfolding force, and corner velocity. It is therefore justified to use HB101 as a model host for single pili force studies since they do not express any native pili that could interfere. In addition, by performing force measurements it is possible to identify pili expressed by bacteria through the characteristic response that each specific variety exhibits.

#### Comparison between different types of pili

In general, class I adhesion pili appear to have the same force-extension response, although different parameter values for bond length, bond strength, and kinetics have been assessed. Previous force-extension results on both P and type 1 pili indicated a major kinetic difference between the two (Andersson et al. 2007). It was shown that the relaxation time of a single pilus from a dynamic regime (50 pN) is  $\sim\!35$  times slower for type 1 than for P pili, i.e., about 7 s compared to 0.2 s, respectively. In addition,  $S_{\rm I}$  pili correlated to UTI (pANN801-13) show  $\sim\!10$  times faster kinetics than P pili and  $\sim\!550$  times faster kinetics than type 1 pili. So far, we do not have any good explanation for why S pili exhibit such fast kinetics.

The dissimilarity in the dynamic response of P and type 1 pili can hypothetically be addressed to the different properties of the flow in the surrounding of a bacteria in vivo. For example, it is known that the urine is transported



in boluses via ureters by peristaltic activity from the kidney to the bladder (Griffiths 1987; Griffiths et al. 1987) and that the bladder expels urine via the urethra (Ozawa et al. 1998). The peristaltic waves in the ureters, which occur at a rate of approximately 3.3 min<sup>-1</sup> (Davenport et al. 2007), generate flow recirculation (Vogel et al. 2004). The flow in the bolus interacting with bacteria thereby results in a high variation of shear rates, as well as perpendicular and reversal wall shear forces (Vogel et al. 2004) similar to those in the ileum (Jeffrey et al. 2003). These forces must be damped by a structure that absorbs and relaxes in a optimum way in order to maintain firm adhesion, i.e., relax fast to minimize the load of the adhesin and thereby extend the lifetime of a slip bond, such as the adhesin of P pili (Björnham et al. 2009), or slow, to maintain the load at reasonable levels for a catch bond, such as the adhesin of type 1 pili (Forero et al. 2006; Nilsson et al. 2006; Thomas et al. 2002). Since it is hypothesized that the adhesin and the rod have coevolved, it is likely that the rod evolved to optimize the function of the adhesin. Therefore, it might be possible that the relaxation behavior of the aforementioned pili could be addressed to the lifetime of such adhesins. It thereby remains as a future work to characterize the properties of the S pili adhesin.

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