

CEST MRI to contrast chondrosarcoma tumors: two contrasts in one acquisition.

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Synopsis

This study aims to develop a non-invasive CEST MRI method to evaluate simultaneously pH and glycoaminoglycans (GAG) as a new imaging method for assessing hypoxic and chondrogenic status in chondrosarcoma *in vivo*.

Introduction

Chondrosarcoma is a malignant tumor of cartilage characterized by a chondrogenic-rich extracellular matrix, *i.e.* poorly vascularized and rich in proteoglycans (PGs)¹. These characteristics make this tumor both chemo and radio-resistant and thus difficult to cure. The development of new bispecific strategies which targets these two main characteristics offer a new approach to specifically target cytotoxic agents. The strategy consists in linking a vector (a quaternary ammonium which targets PG^{2,3,4} to a hypoxia-activated prodrug⁵. If the hypoxic status of the tumors can be assessed by nuclear imaging with ¹⁸F MISO⁶ and proteoglycan status by ⁹⁹mTc NTP 15-5 scintigraphy^{7,8,9} it requires however 2 separated acquisitions. Furthermore, the accuracy of these methods is still highly discussed. In this context we propose to develop an MR strategy based on Chemical Exchange Saturation Transfer (CEST) to simultaneously co-register both hypoxia (by assessing pH) and PGs (by quantifying glycoaminoglycans (GAG) content). The relevance of CEST MRI method will be validated in regards of standard MRI techniques to estimate pH and GAG concentration *in vivo*, *i.e.* by ³¹P MRS¹⁰ and ²³Na MRI¹¹, respectively.

Methods

In vitro study: The work hypothesis was first tested in a Chondroitin sulfate A (type of GAG) phantom at different concentrations (1, 2.5, 5 and 10mg/mL) and a creatine phantom (50mM) at several pHs (6, 6.5, 7, 7.5).

In vivo study: NUDE mice (n=12) were implanted with HEMC-SS cells (human chondrosarcoma) in contact to tibia. Tumors were then allowed to growth for 7 weeks. MRI images were acquired at 11.7 T on a Bruker BioSpec117/16USR using a 40-mm quadratic volume coil. First, DWI imaging of chondrosarcoma was performed (20 slices, TR/TE=2000/26 ms; b = 500s/mm²; spatial resolution=0.1x0.1x1 mm³), then WASSR (B₁=0.1μT for 1.5 sec, with saturation frequencies ranging from Δω=-260 Hz to 260Hz, BW=50Hz, spatial resolution=0.5x0.5x1 mm³) and CEST Z-spectra (B₁=1.5μT for 4 sec, with saturation frequencies ranging from Δω=-2500 Hz to 2500Hz, BW=50Hz, spatial resolution=0.5x0.5x1 mm³) were acquired with EPI based sequences. ³¹P MRS was performed thanks to a volume coil while ²³Na imaging was recorded by using a 20-mm surface coil.

Data analysis: CEST data were analyzed using an in-house program written in Matlab® R2017a. Briefly, CEST analysis was performed on ROI(s) drawn around the chondrosarcoma. After correction for B₀ inhomogeneity, the CEST maps were generated.

Results

Variations in GAG concentration (fig. 1) and in pH (fig. 2) were observed *in vitro* by CEST MRI by monitoring the magnetization transfer ratio asymmetry at 450 and 1000Hz, respectively.

In vivo (Fig. 3), we observed an increase of asymmetry at 450Hz in the chondrosarcoma associated with the high PGs content. The asymmetry of the signal at 450Hz should increase with the pathology development. *In vivo*, in the z-spectrum we observed a reduction of asymmetry at 1000Hz in the chondrosarcoma associated with acidosis in the hypoxic core. Validation of these results by using well-accepted MRI/MRS methods is in progress.

Discussion

The phantom study demonstrated that CEST effect is sensitive to both the hydroxyl (at 450Hz ppm from the water frequency) and amino (at 1000Hz) groups. These moieties allow extracting the GAG concentration and the pH, respectively. If GAG CEST MRI can be used to monitor the cartilage degradation in arthrosis¹² by monitoring other exchangeable protons CEST MRI offers the possibility to obtain simultaneously several contrasts. Chondrosarcoma is a tumor combining both GAG concentration changes as well as pH evolution. By recording a full z-spectrum on a window from + 5 to - 5 ppm, GAG concentration and hypoxia status were simultaneously co-investigated in chondrosarcoma tumor. If the GAG content can be easily assessed *in vivo*, CEST signal from -NH moieties required more investigations because of the endogenous mobile proteins and peptides present *in vivo* which induce a negative background and reduce the signal detected during asymmetry analysis of z-spectra¹³. The two CEST images are currently being validated by ²³Na imaging (GAG concentration) and ³¹P MRS (pH).

Conclusion

CEST MRI can be used as a new strategy for non-invasive assessment of chondrosarcoma. CEST MRI offers the possibility to assess in the same exam the 2 main characteristics of this tumor: pH and GAG content. CEST MRI is able to identify and differentiate zones of hypoxia *in vivo*. After the validation of the method, our next steps are (i) to compare CEST and nuclear images and (ii) to non-invasively evaluate drug therapeutic

efficiency thanks to CEST MRI.

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Figures

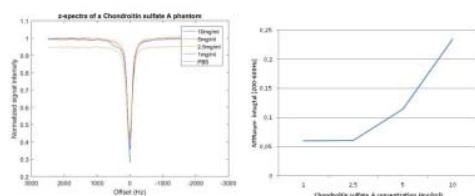


Fig. 1. Z-spectra of a chondroitin sulfate A (i.e a GAG unit) phantom at 4 different concentrations (10, 5, 2.5 and 1 mg/ml) (left). MTR asymmetry as function of chondroitin sulfate A concentration (right). Contrast observed at around 450Hz is associated to –OH function of GAG.

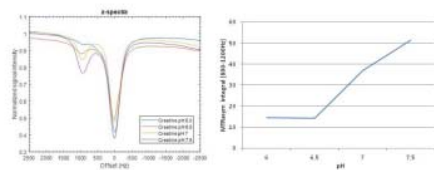


Fig. 2. Z-spectra (left) of a 50mM creatine phantom at 4 different pH (6.0, 6.5, 7.0, 7.5). MTR asymmetry as function of pH (right). pH contrast is obtained around 1000Hz.

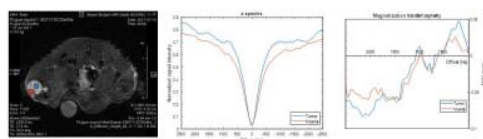


Fig. 3. CEST MRI in vivo. DWI (left) of one mouse with chondrosarcoma (blue circle). z-spectra (middle) and MTR asymmetry (right) obtained from ROI localized in blue for tumor and red for paw muscle. Differences in MTR asymmetry can be observed between structures. Increase of asymmetry at 250Hz may reflect the high GAG contain reduced asymmetry is also observed at 1000Hz in the z-spectra reflecting the acidosis in the tumor core however the negative background reduce the signal signal detected when asymmetry analysis of z-spectra is used to quantify this effects *in vivo*.