

Everything you always wanted to know about RF bias correction ... but were afraid to ask

Sylvie Clerjon, Jean-Marie Bonny
Centre INRA de Clermont-Ferrand Theix, France



FOODMR 2014 – Cesena, Italy
Thursday 22 May 2014



Spin density measurement affected by RF bias and noise

Spin density weighted imaging

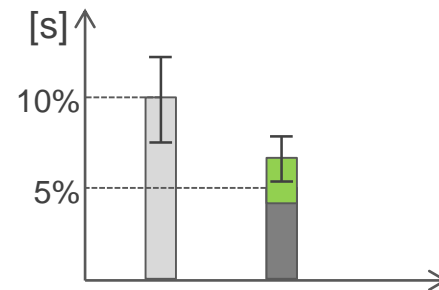
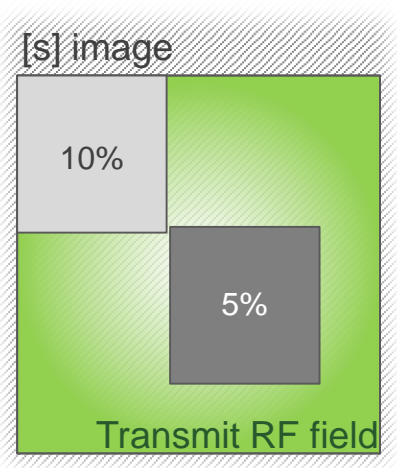
Measured signal

RF bias

$$S \propto [s] \cdot w_1^- \cdot M_{x,y}(w_1^+)$$

Spin density,
what we want
to measure

A particular case: *Spin Density Map*
where $M_{x,y}(w_1^+) = 1$



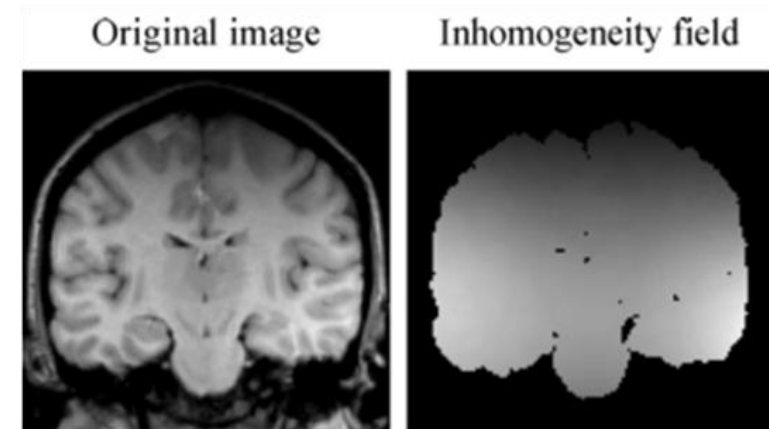
What we can expect concerning coils homogeneity

Manufacturers

→ difficult to find quantified information

Bibliography

In brain transmit RF field bias = w_1^+ variation 30%



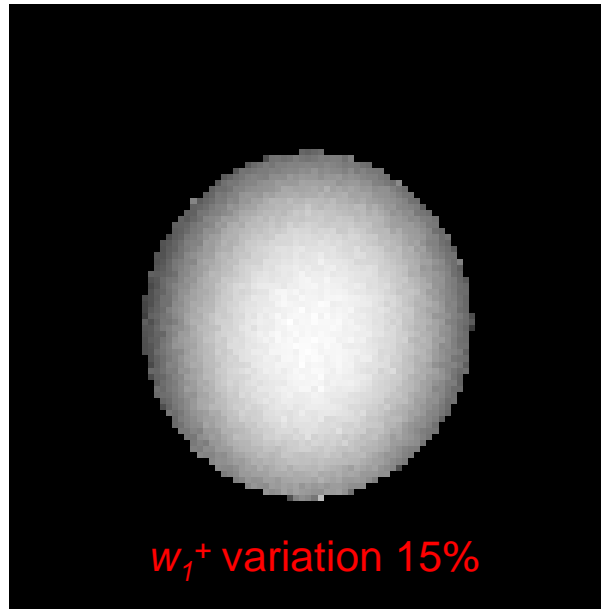
Vovk et al. (2007). A review of methods for correction of intensity inhomogeneity in MRI. *Ieee Transactions on Medical Imaging*, 26(3), 405-421.

What we can expect concerning coil homogeneities

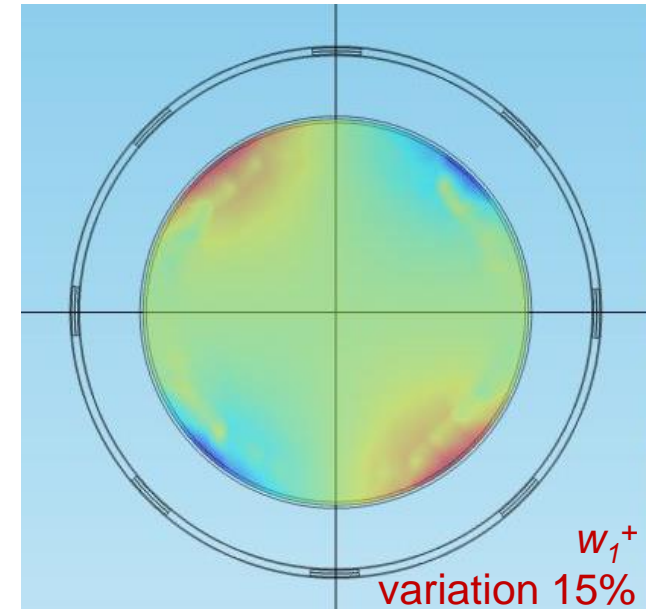


Our own experiments and simulation

Rapid Biomedical 19 cm birdcage coil. Bruker Biospec 4,7T. Prescribed angle 60°. Sample: 6 cm diameter homogeneous gelatin cylinder



Numerical simulation, birdcage



What we can expect concerning coil homogeneities

Spatial variations of transmit RF field can reach 40%

Spatial variations depend on

- Coil geometry
- Sample (size, shape, dielectric properties)
- Frequency : High field \rightarrow high RF frequency \rightarrow small wavelength / sample size \rightarrow high heterogeneities
- Nucleus

Food science needs quantitative imaging of spin density:

- Products characterization
- Drying, cooking: water mapping
- Salting: sodium mapping

RF bias must be avoid for food quantitative imaging of spin density

1. RF field w_1^+ mapping
2. Image correction

Mapping transmit RF field

DAM-SP for Double Angle Method – Selective Pulse

Principle :

Independent on
receive field

$$\frac{S(k.w_1^+)}{S(w_1^+)} \propto \frac{[s].w_1^-}{[s].w_1^-} \cdot \frac{M_{x,y}(k.w_1^+)}{M_{x,y}(w_1^+)}$$

The ratio of two
magnitude images
at two different
prescribed angles

Independent
on spin density

The map only depends
on transmit field

DAM-SP versus DAM

- No bias in $M_{x,y}$ model due to pulse shape
- Can be used in SE imaging
- 2D

Bouhrara M, Bonny JM. B1 mapping with selective pulses. Magnetic Resonance in Medicine (2012) DOI: 10.1002/mrm.24146.

The DAM-SP's 3 experimental parameters



k factor between the two prescribed angles

Have to be optimized

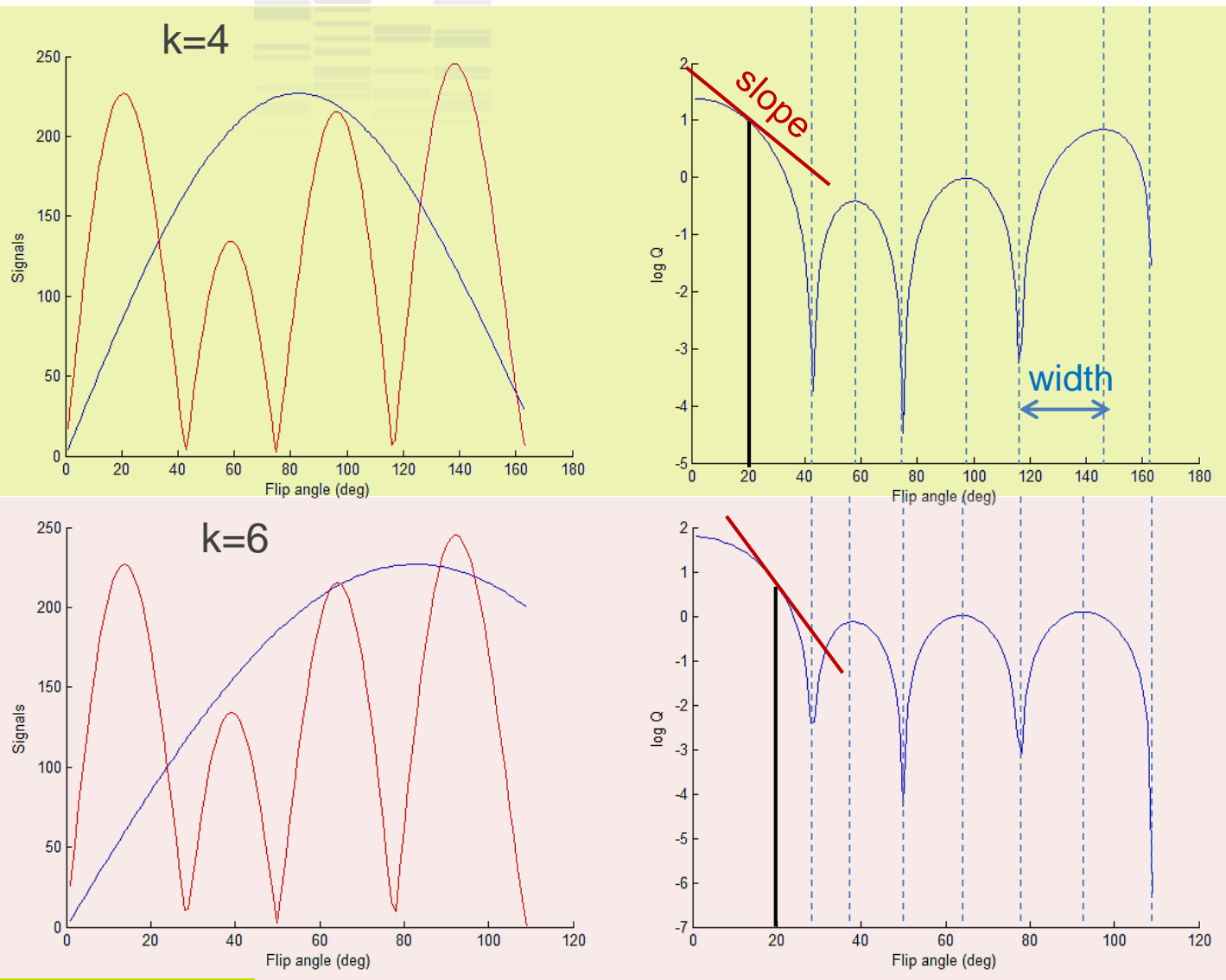
Pulse shape governing $M_{x,y}(w_1^+)$

We choose a Shinnar-Le Roux (SLR) pulse

MRI sequence

We used a Flash

Optimizing the k factor



Width = range

Slope = sensitivity

Depends on the pulse

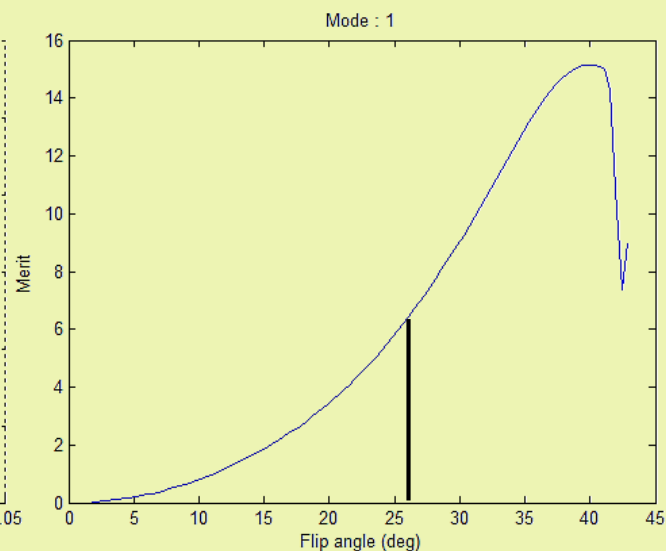
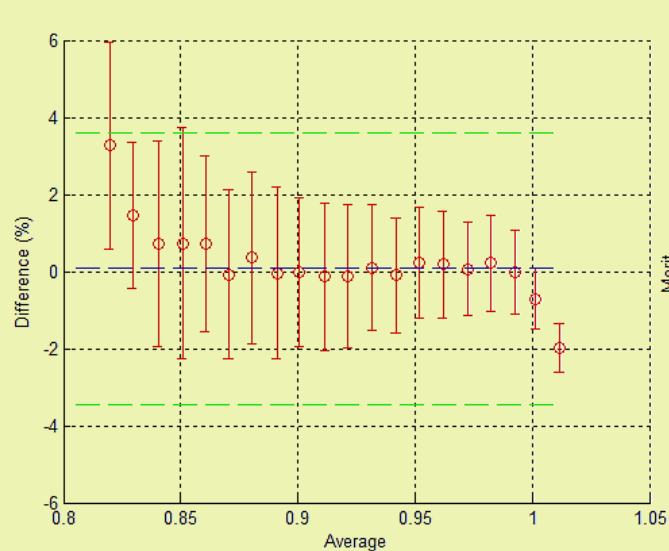
Optimizing the k factor

Measurements on an homogeneous phantom, Flash,
Bruker Biospec 47/40, quadrature birdcage coil

k=4



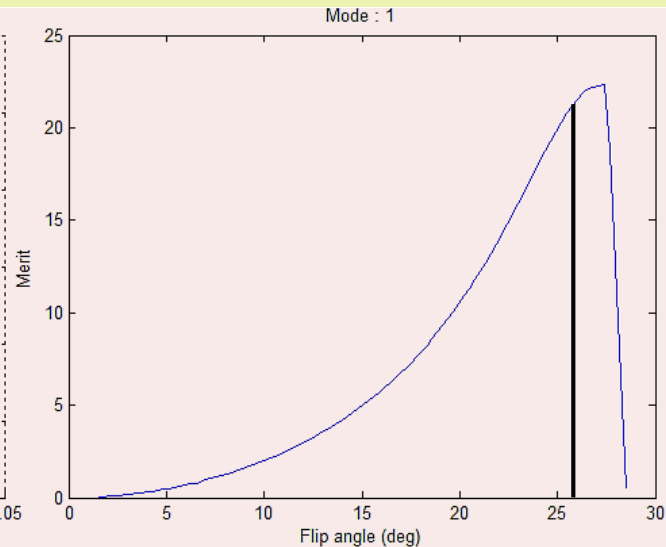
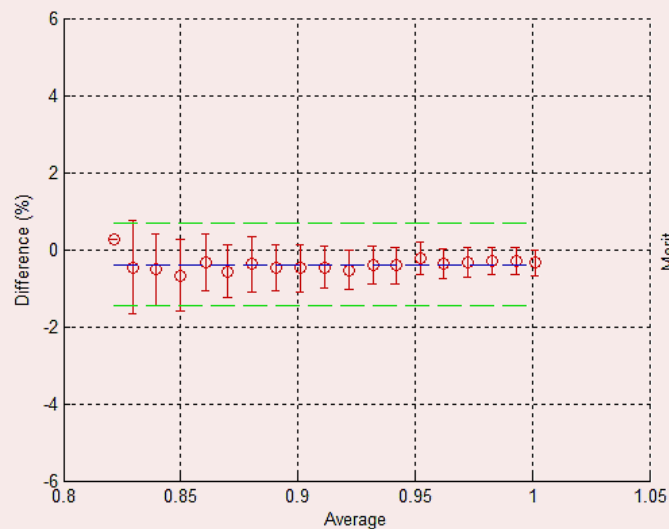
Transmit RF field map



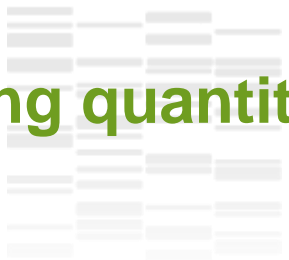
k=6



Transmit RF field map



Correcting quantitative image from transmit RF field w_1^+ bias



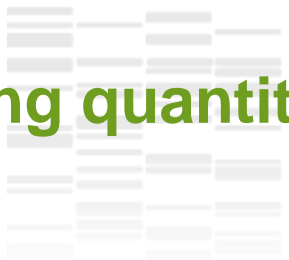
We have an accurate RF field w_1^+ map



How to correct our images ?

$$S^* \propto \frac{[s] \cdot w_1^- \cdot M_{x,y}(\widehat{w_1^+})}{\widehat{w_1^-}}$$

Correcting quantitative image from transmit RF field w_1^+ bias



We have an accurate RF field w_1^+ map



How to correct our images ?

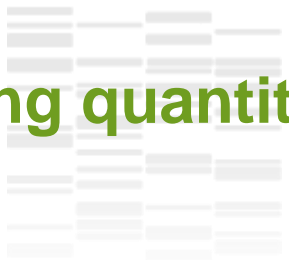
We have to be sure $w_1^- = w_1^+$

$$S^* \propto \frac{[s] \cdot w_1^- \cdot M_{x,y}(\widehat{w_1^+})}{\widehat{w_1^+}}$$

Single coil

Always equal?

Correcting quantitative image from transmit RF field w_1^+ bias



We have an accurate RF field w_1^+ map



How to correct our images ?

We have to be sure $w_1^- = w_1^+$

$$S^* \propto \frac{[s] \cdot w_1^- \cdot M_{x,y}(\widehat{w_1^+})}{\widehat{w_1^+} \cdot M_{x,y}(\widehat{w_1^+})} \propto [s] \cdot \frac{w_1^-}{w_1^+} \propto [s]$$

Single coil

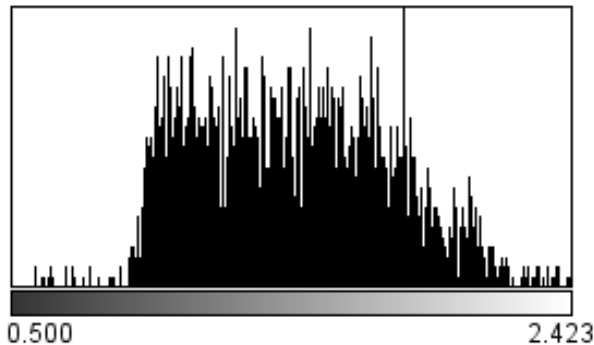
Always equal?

Correcting quantitative image from transmit RF field w_1^+ bias

Measurements on an homogeneous phantom diam. 6 cm, Flash, Bruker Biospec 47/40, quadrature birdcage coil diam. 19 cm



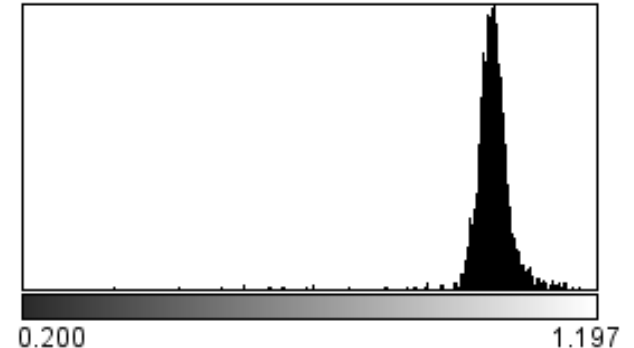
Signal spatial variation 75%



Correction

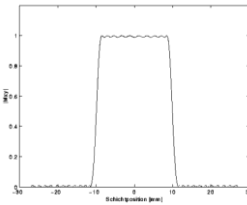


Signal spatial variation 4%

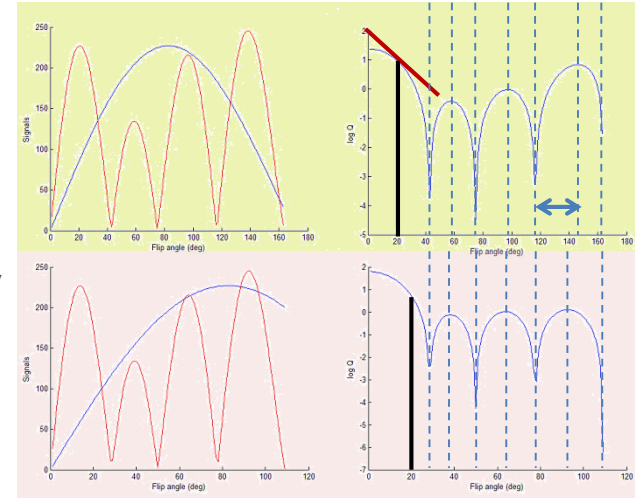


Summarized guide

Choose a pulse



Compromise between measurement range and sensitivity
best polarization point and best k factor for
the best w_1^+ map



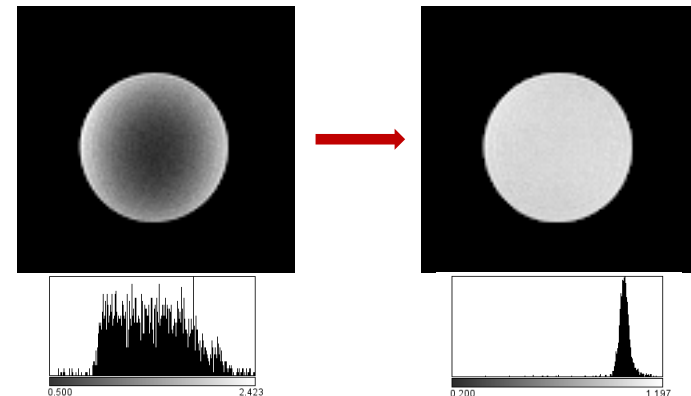
Perform acquisitions at prescribed flip angle and k.prescribed flip angle

Compute w_1^+ map



Correct your raw density weighted images by dividing
them by signal due to w_1^+

You obtain quantitative images



Discussion

Transmit and receive RF fields equality (amplitude and phase)

Sample

Dielectric properties (anisotropy, hydration, conductivity due to salt...)

Shape and size

Coil

Near field behavior close to coil conductors → position in coil

Knowing their coils: **area of fields equality**

Coils designers have to work on this parameter

Noise

Regularization before computing (in DAM-SP and for RF field correction)

Optimizing acquisition protocol to improve SNR

DAM-SP on each sample before quantitative imaging

w_1 mapping. How and why?



The MRI experiments were performed at the MR Platform for Biological Systems, INRA Center of Clermont-Ferrand, France.



Thanks to my colleagues,
Jean-Marie Bonny

Thanks for your attention